

A preliminary study on the synthesis and characterisation of dopamine-grafted block copolymers

Irada MAMADOVA¹, Buse AVCI², Pınar Sinem OMURTAG ÖZGEN^{3*}

¹ Marmara University, Institute of Health Sciences, Department of Basic Pharmacy Sciences, Istanbul, Türkiye

² Bezmialem Vakıf University, Institute of Life Sciences and Biotechnology Institute, Department of Biotechnology, Istanbul, Türkiye

³ Marmara University, Faculty of Pharmacy, Department of Basic Pharmacy Sciences, Istanbul, Türkiye

ABSTRACT

Biodegradable and biocompatible polymers are increasingly gaining importance in biomedical applications. Herein, we report the development of a thermoresponsive and tissue-adhesive platform based on a block copolymer of poly(N-isopropyl acrylamide) (P(NIPAM)) and polydopamine, synthesized via RAFT polymerization. Following the synthesis of P(NIPAM) homopolymer, P(NIPAM) was used as a macro-RAFT agent to incorporate the aldehyde block of the copolymer. The presence of aldehyde groups in the block copolymer was exploited to attach dopamine via imine chemistry. Spectroscopic and chromatographic techniques confirm the structures of intermediate compounds and polymers. The dopamine release profile of the copolymer was monitored for 72 hours at pH 7.4, and the total amount of dopamine released was found to be 53%. The synthesis of a dopamine-grafted block copolymer, which combines PNIPAM's thermoresponsive properties with dopamine's surface adhesion capabilities, suggests this platform could be a promising material for various future applications, such as implant interfaces and antimicrobial applications.

Keywords: polydopamine, RAFT polymerization, biocompatible materials

* Corresponding author: Pınar Sinem OMURTAG ÖZGEN

E-mail: sinem.ozgen@marmara.edu.tr

ORCID:

Irada MAMADOVA: 0009-0005-7103-216X

Buse AVCI: 0000-0002-0302-9429

Pınar Sinem OMURTAG ÖZGEN: 0000-0003-2493-9664

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INTRODUCTION

Dopamine (DA, 3,4-dihydroxyphenylethylamine) is an important neuromodulator molecule produced by animals and plants. Dopamine plays a part in many body functions, and changes in dopamine levels in the body are linked to many diseases¹.

In recent years, polydopamine (PDA), synthesized either by polymerizing dopamine-based monomers or by grafting dopamine into the functional group of a polymer backbone, has vital use owing to its significant properties, including its photothermal properties, redox capabilities, coating, and natural antibacterial and surface adhesion characteristics²⁻⁶. All these properties are related to the chemical structure of dopamine, specifically the catechol and primary amino groups⁷. The synthesis of dopamine-based polymers requires further investigation due to their potential as promising biocompatible and antimicrobial materials in material science and biotechnology^{8,9}.

Controlled “living” radical polymerization (CLRP) techniques promote controlled chain growth, maintain active chain ends, and enable chain re-growth as needed¹⁰. The molecular weight, distribution, and functionality of polymers can be controlled through CLRP techniques. The primary CLRP techniques are atom transfer radical polymerization (ATRP), reversible addition-fragmentation chain transfer (RAFT), and nitroxide-mediated polymerization (NMP)¹¹. CLRP is also widely used to obtain complex macromolecular structures such as blocks, stars, and grafts. CLRP’s architectural control and functionalization capacity have an impact on the usage of these methods in biomedical applications, surface coatings, and nanotechnology¹². RAFT polymerization is one of the most preferred CLRP techniques because it enables the synthesis of polymers with a predefined, narrow molecular weight range and polydispersity, possessing the desired structural properties^{13,14}. Moreover, RAFT polymerization is crucial for tailoring the design of polymer-based advanced biomaterials.

In recent years, biodegradable and biocompatible polymers have gained significant attention in both biomedical applications and materials science¹⁵. Biodegradable polymers interact with biological molecules and are used in various applications, including drug delivery and tissue engineering¹⁶. These polymers degrade in the body over time, producing harmless byproducts. These features make them preferred in treatment methods that require controlled drug release¹⁷.

Using RAFT polymerization, different polydopamine (PDA) polymers can be synthesized either by directly polymerizing dopamine monomers or by the conjugation of dopamine molecules into the polymer's main chain through its functional groups (post-modification)¹⁸⁻²¹. The applications of PDAs can be enlarged by combining polymers with different properties (hydrophobic, hydrophilic, thermoresponsive, etc.) using different architectures such as block, star, and graft copolymers⁷.

A temperature-sensitive polymer, poly(*N*-isopropyl acrylamide) (P(NIPAM) or PNIPAAm), is an important smart polymer that can change the conformation of its polymer chains by changing temperature. So, this property makes P(NIPAM) an excellent choice for the synthesis of temperature-sensitive systems in biomedical applications^{22,23}.

In a study by Mocan et al., a series of polystyrene-*b*-poly(*N*-isopropyl acrylamide) (PS-*b*-PNIPAM) block copolymers were synthesized via RAFT polymerization. Subsequently, innovative nanoporous membranes with fully temperature-controllable permeability were produced using the self-assembly and non-solvent induced phase separation (SNIPS) methods for these copolymers. As a result, it was determined that the permeability increased by almost 400% when the temperature rose from room temperature to 50°C, and this thermo-responsive characteristic was fully reversible²⁴. In another study, micelles prepared from the amphiphilic block copolymer poly(*N*-isopropylacrylamide-*co*-acrylamide)-*b*-poly(*n*-butyl methacrylate), containing the poorly water-soluble anticancer drug methotrexate, were shown to achieve drug release and exhibit efficacy against cancer cells when combined with localized hyperthermia^{25,26}. Furthermore, PNIPAM-protein-based conjugates were utilized for thermally controlled on-off switchable protein release owing to PNIPAM's lower critical solution temperature (LCST) behavior²⁷.

In a 2017 study by Zhang et al., a thermoresponsive surface was developed for culturing and harvesting human mesenchymal stem cells (hMSCs) by depositing PNIPAAm onto polydopamine (PDA) coated cell culture substrates. hMSCs were cultured on the prepared PNIPAAm-*g*-PDA coated surface and harvested by switching from physiological to ambient temperature. The results showed that hMSCs could detach from the PNIPAAm-*g*-polydopamine surface after the temperature was lowered. Furthermore, the detached hMSCs were able to proliferate on the PNIPAAm-*g*-PDA coated surface for further growth and harvest. The study presented the synthesis of a biocompatible and thermoresponsive surface for hMSCs that can be harvested²⁸.

Combining materials like polydopamine (PDA) and poly(*N*-isopropyl acrylamide) (PNIPAM) enables the development of specific applications, such as antimicrobial coatings, targeted drug delivery, and biosensor systems. Despite this progress, further research is still needed to develop these systems. Although few examples of PNIPAM-*b*-PDA block copolymer synthesis via RAFT polymerization exist, our study employs a different strategy¹⁸⁻²¹. Instead of conventional dopamine-based monomers, dopamine was grafted to the polymer using pH-sensitive imine bonds. This approach not only facilitates tunable control over the amount of conjugated dopamine but also the amount of dopamine conjugated to the polymer can be adjusted in a controlled manner.

For this purpose, herein we employed RAFT polymerization to synthesize p-(2-methacryloxyethyl)benzaldehyde (MAEBA) and *N*-isopropylacrylamide block copolymers. Grafting of dopamine was then achieved via pH-sensitive imine bonding between the free aldehyde groups in the MAEBA block and the amine groups in the dopamine molecule. The chemical structure of the resulting dopamine-grafted copolymer was thoroughly characterized using spectroscopic and chromatographic methods. Finally, the dopamine release of this block copolymer at the physiological pH of 7.4 over a 72-hour period was investigated.

METHODOLOGY

Chemicals

Dopamine hydrochloride ($\geq 98\%$ (TLC)), 4-hydroxybenzaldehyde (98%), 2-bromoethanol (95%), methacryloyl chloride (97%, contains monomethyl ether hydroquinone as a stabilizer), triethylamine ($\geq 99.5\%$, Et₃N), *N*-isopropylacrylamide (NIPAM, $\geq 99\%$), chloroform-*d* (CDCl₃), dimethyl sulfoxide-*d*₆, phosphate buffered solution (PBS), potassium carbonate (for analysis EMSURE® ACS, ISO, Reag. Ph. Eur.), toluen (ACS reagent, $\geq 99.5\%$), tetrahydrofuran ($\geq 99.9\%$, anhydrous, contains 250 ppm BHT as inhibitor, THF), acetonitrile (EMPLURA®, CH₃CN), and dimethylsulfoxide (ACS reagent, $\geq 99.9\%$, DMSO) were purchased from Sigma-Aldrich; dichloromethane (Ph. Eur., NF, DCM), hexane (extra pure), and diethyl ether (BP, Ph. Eur) were purchased from ISOLAB and all chemicals were used as received. Azobisisobutyronitrile (AIBN) and *N*-isopropylacrylamide were purified by crystallizing in ethanol, and then they were dried overnight at 25°C in a vacuum oven to remove the inhibitor separately.

Butyl 2-cyanopropan-2-yl-carbonotrichioate (CBPA) and aldehyde functional monomer (MAEBA, p-(2-methacryloxyethoxy)benzaldehyde) were synthesized according to a published procedure^{29,30}.

Instruments

Nuclear magnetic resonance (NMR) spectra were acquired with a Bruker BioSpin AG Avance 500 MHz spectrometer (^1H : 500 MHz, ^{13}C : 125 MHz) in CDCl_3 and $\text{DMSO}-d_6$ solvents. All chemical shifts are expressed in ppm (δ) relative to $\text{Si}(\text{CH}_3)_4$ ($\delta=0$ ppm) as an internal standard. The average molecular weight (M_n) and the molecular weight distribution index (PDI) (M_w/M_n) of the polymers were determined using a Viscotek GPCmax Gel Permeation Chromatography (GPC) instrument. A mobile phase of HPLC-grade tetrahydrofuran (THF) containing 0.05% butylated hydroxytoluene (BHT) was pumped at a rate of 1 mL/min and maintained at 35 °C. Polymer solutions, prepared in THF at a concentration of 4-5 mg/mL, were injected in 50 μL aliquots. Narrow-polydispersity polystyrene (PS) standards from Polymer Laboratories were used for calibration. The Bruker Alpha model was used for the FT-IR analyses. UV spectra were obtained using a Hitachi U-2900 UV-Vis spectrophotometer.

Synthesis of poly(N-Isopropylacrylamide) homopolymer (P(NIPAM))

Butyl 2-cyanopropan-2-yl-carbonotrithioate (CBPA) as the RAFT agent (17 mg, 0.058 mmol), NIPAM (0.5 g, 4.0 mmol), and azobis(isobutyronitrile) (AIBN, 1.2 mg, 0.007 mmol) were added to a septum-sealed flask and dissolved in 4.4 mL toluene³¹. The ratio of polymerization was determined as $[\text{M}]_0/[\text{RAFT-agent}]/[\text{AIBN}]=75:1:0.125$. The flask was placed in an ice bath, and nitrogen gas was passed through the reaction mixture for 45 minutes. Then, the reaction was placed in the oil bath pre-set to 70 °C and stirred at 400 rpm for 17 hours. After 17 hours, the seal of the flask was opened to the air environment. The polymerization solution was concentrated by partially evaporating the toluene, and the polymer in the flask was precipitated in a beaker with 10 times more hexane to remove the unreacted monomer and the RAFT agent. The purified polymer was then dried under vacuum overnight.

Block copolymer synthesis, poly(N-Isopropylacrylamide)-block-poly(p-(2-methacryloxyethoxy)benzaldehyde) (P(NIPAM-b-MAEBA))

The molecular weight of the P(NIPAM) homopolymer was determined as 4.36 kDa by using ^1H NMR analysis. 96 mg of homopolymer, 0.25 g (1.1 mmol) of p-(2-methacryloxyethoxy)benzaldehyde (MEABA) monomer, and 0.55 mg (3.3 mmol) of AIBN were weighed. They were added into a septum-sealed flask and dissolved in 1.65 mL toluene. The molar ratio of polymerization $[\text{M}]_0/[\text{MacroRAFT-agent}]/[\text{AIBN}]$ was set to 50:1:0.150. The flask was placed in an ice bath, and nitrogen gas was passed through the reaction mixture for 45

minutes. The reaction was then placed in an oil bath pre-set to 70°C and stirred at 400 rpm for 18 hours. After 18 hours, the seal of the flask was opened to the air environment. The polymerization solution was concentrated by partially evaporating the toluene, and the block copolymer in the flask was precipitated in a beaker with 10 times more diethyl ether to remove the unreacted monomer and the precursor homopolymer and centrifuged. This process was done twice in total. The obtained polymer was dried overnight in a vacuum oven. The average molecular weight (M_n) of the copolymer was determined by gel permeation chromatography (GPC), and the $M_{n,NMR}$ value was determined by 1H NMR analysis.

Grafting of dopamine to block copolymer

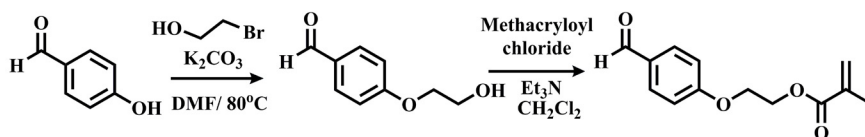
40 mg (0.0033 mmol) of block copolymer was dissolved in a DMSO/water (4/1, v/v) solution mixture. 20 mg of dopamine.HCl (0.13 mmol) was weighted to be 1.2 times the amount needed for the repeating aldehyde units in the copolymer, and 46 μ L of triethylamine (0.27 mmol) was added to the mixture, which was stirred for 20 hours at room temperature to increase the amount of dopamine. Then, the mixture was transferred to the dialysis membrane (MWCO=3500) and dialyzed against deionized water, changing the water every 6 hours. The dispersion in the membrane was then lyophilized and stored at +4°C for future use.

***In vitro* dopamine release assay**

The release of dopamine was measured using the dialysis method. The experiment was conducted in triplicates. 50 mg of dopamine-conjugated copolymer dissolved in 3 mL of distilled water and then transferred into the dialysis bag and incubated at 37°C in 50 mL of phosphate-buffered saline solution (PBS, pH 7.4). A 1 mL sample was taken at specific intervals (0.5, 2, 4, 8, 10, 24, 48, 56, and 72 h) over 72 hours, and the same amount of fresh medium was added at each interval. The amount of dopamine released from the samples was determined using a previously prepared calibration curve of dopamine, and the maximum absorbance value was measured at 280 nm with a UV-Vis spectrophotometer. Dopamine cumulative release percentages were calculated using the obtained data. Then, the cumulative percentages of dopamine release were plotted against time.

RESULTS and DISCUSSION

For synthesizing block copolymer, an aldehyde functional monomer (p-(2-methacryloxyethoxy)benzaldehyde, MAEBA) were first prepared according to previously described in the literature²⁹ (Scheme 1).



Scheme 1. Synthetic pathway for (p-(2-methacryloxyethoxy)benzaldehyde (MAEBA)

In the first step p-(2-hydroxyethoxy)benzaldehyde (PEHBA) compound was synthesized. The existence of the characteristic functional groups of PEHBA was confirmed by ^1H NMR, with signals at 2.67 ppm for the hydroxyl group, at 4.01 and 4.16 ppm for the methylene protons, at 7.84 and 7.03 ppm for the phenyl group, and at 9.87 ppm for the aldehyde proton (Figure 1).

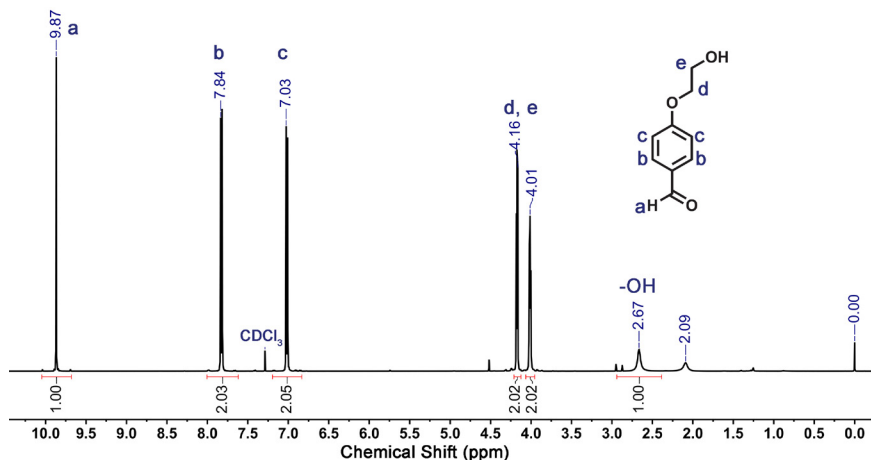


Figure 1. ^1H NMR spectrum of p-(2-hydroxyethoxy)benzaldehyde in CDCl_3

Secondly, p-(2-methacryloxyethoxy)benzaldehyde (MAEBA) was synthesized by using a precursor molecule (PEHBA). The existence of the characteristic functional groups of MEABA was confirmed by ^1H NMR with the signal at 1.96 ppm for methyl group, at 4.33 and 5.53 ppm for methylene protons, at 5.61 and 6.15 ppm for double bond, at 7.05 and 7.85 ppm for the aromatic group, and the signal at 9.91 ppm denotes the aldehyde proton (Figure 2).

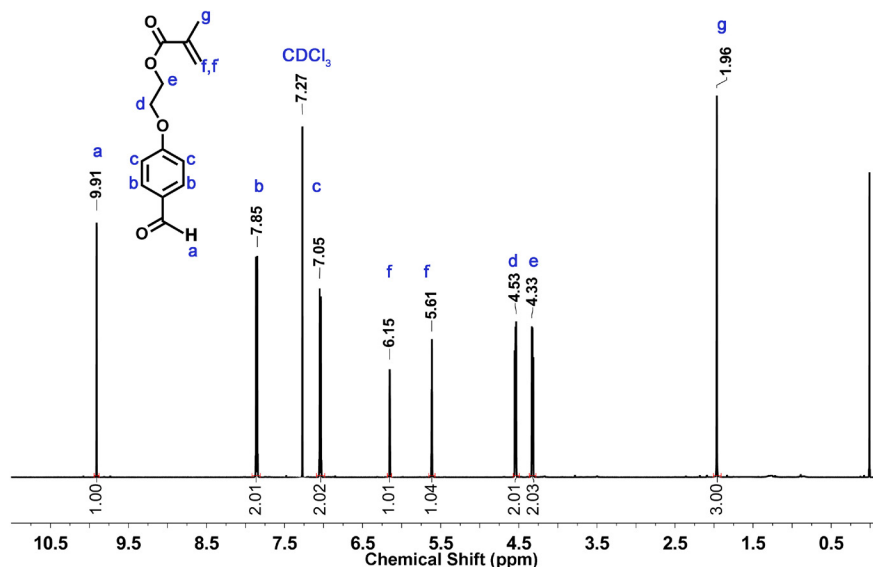
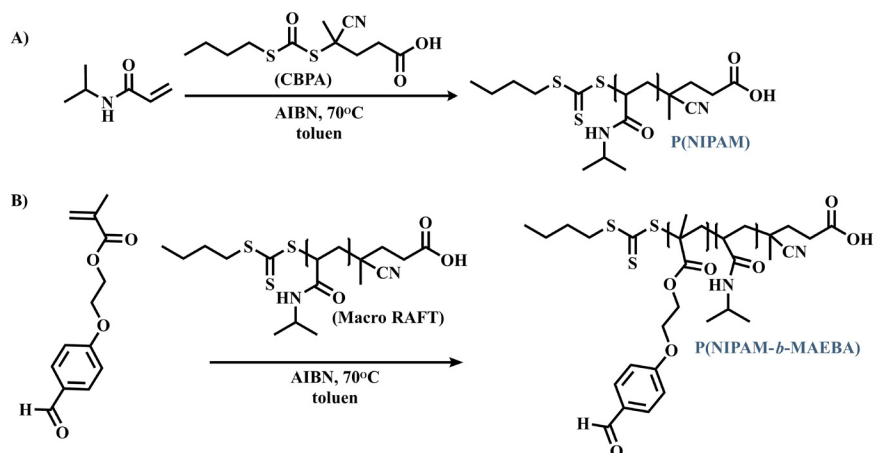


Figure 2. ¹H NMR spectrum of p-(2-methacryloxyethoxy)benzaldehyde in CDCl₃

A two-step sequential RAFT polymerization procedure was then employed to obtain an aldehyde-functional block copolymer. Briefly, CBPA chain transfer agent (RAFT Agent) was used to obtain a Poly(*N*-isopropyl acrylamide) homopolymer, which was then used as a Macro-RAFT agent to polymerize the monomer of MAEBA. The P(*N*-isopropylacrylamide) (P(NIPAM)) homopolymer was synthesized at a molar ratio of $[M]_0/[RAFT \text{ agent}]/[AIBN]=75:1:0.125$. Polymerization was performed at 70°C for 17 hours (Scheme 2A). After the polymerization was completed, the homopolymer was purified by dissolving it in tetrahydrofuran and then dropping it into cold hexane to remove any leftover monomers and RAFT agents.



Scheme 2. Synthetic pathway for block copolymer by RAFT polymerization

The chemical structure of homopolymer and monomer conversion was determined by ^1H NMR spectrum shown in Figure 3A. The degrees of polymerization (DPs) of the P(NIPAM) was found to be 36 by comparing the integration of the signal of methylene protons in $-\text{CH}_2-\text{S}-\text{C}=\text{S}$ at 3.36 ppm from the RAFT agent and the amide proton at 6.43 ppm in the polymer backbone (Figure 3A).

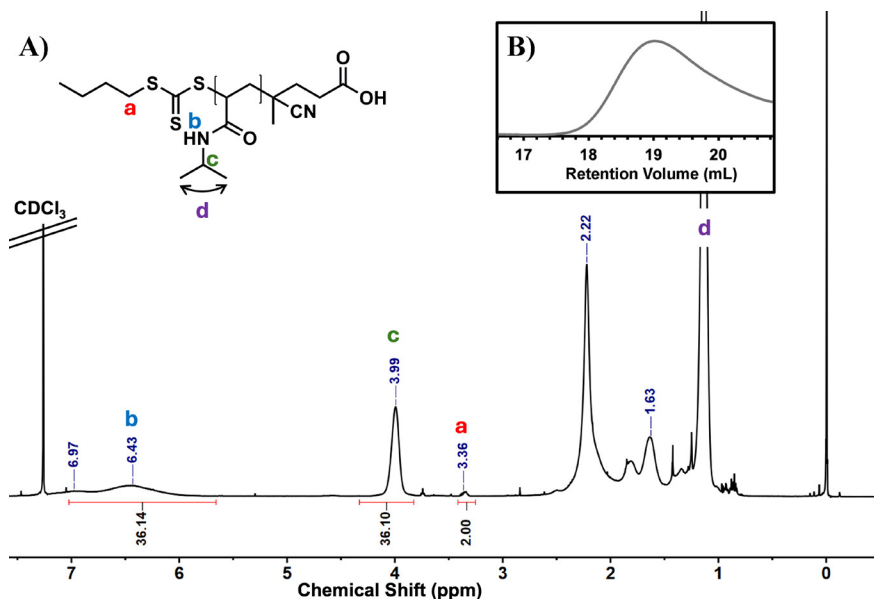


Figure 3. A) ^1H NMR spectrum of P(NIPAM) in CDCl_3 , B) GPC chromatogram of P(NIPAM)

The $M_{n, \text{NMR}}$ was calculated to be 4.36 kDa, whereas the number average molecular weight ($M_{n, \text{GPC}}$) was found to be 1.32 kDa, with an M_w/M_n ratio of 1.25 (Figure 3B, Table 1).

Subsequently, the homopolymer was used as a Macro-RAFT agent to extend the MAEBA block of the copolymer in the presence of AIBN and MAEBA monomer in toluene for 18 h (Scheme 2B) with a ratio $[M]_0:[\text{RAFT agent}]:[\text{AIBN}]=50:1:0.15$. Comparison of ^1H NMR spectra of homopolymer P(NIPAM) and P(NIPAM-*b*-MAEBA) demonstrated the successful synthesis of P(NIPAM-*b*-MAEBA). Figure 4A shows new signals at 9.80, 7.74, and 6.92 ppm assigned to aldehyde and aromatic moieties of the MAEBA units. The DPs of P(NIPAM-*b*-MAEBA) was determined from ^1H NMR end group analysis by comparing the integrals of peaks at 6.39 (-NHC=O of P(NIPAM)) and with 9.80 ppm (aldehyde protons of P(MAEBA)), which were calculated as 33. The $M_{n, \text{NMR}}$ was calculated to be 12.09 kDa, whereas the number average molecular weight ($M_{n, \text{GPC}}$) was found to be 29.45 kDa, with an M_w/M_n ratio of 1.50 (Figure 4B, Table 1).

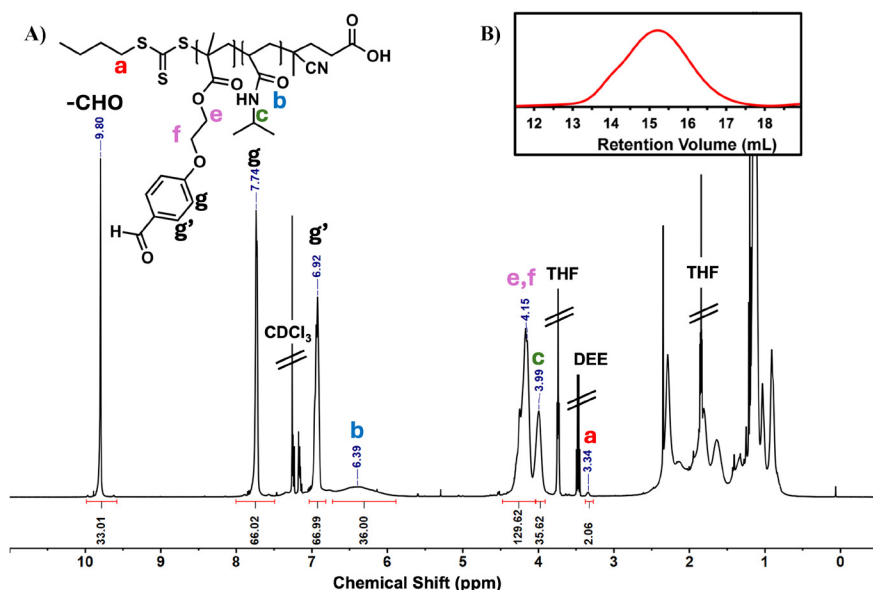
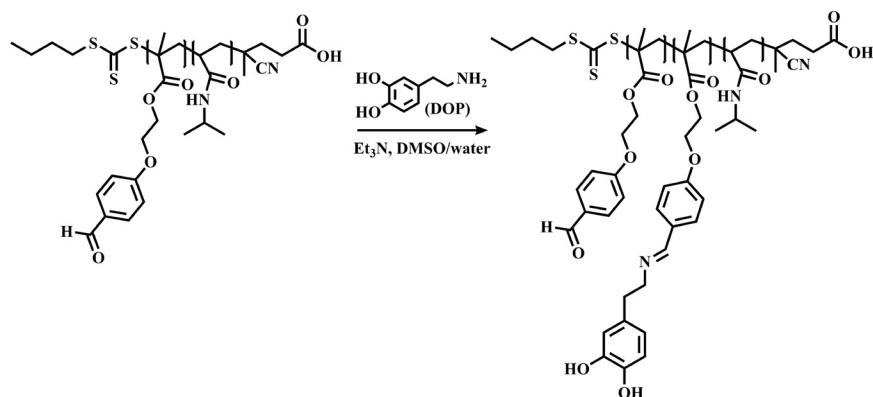


Figure 4. A) ^1H NMR spectrum of P(NIPAM-*b*-MAEBA) in CDCl_3 , B) GPC chromatogram of P(NIPAM-*b*-MAEBA)

The aldehyde groups in the backbone of the block copolymer were used to attach amino compounds through a condensation (Schiff base) reaction, forming imine bonds. Dopamine molecules were grafted onto the aldehyde groups of the P(NIPAM-*b*-MAEBA) copolymer backbone in a basic medium (Scheme 3).



Scheme 3. Synthetic pathway for grafting of dopamine to block copolymer

^1H NMR analysis confirmed the successful grafting of eight dopamine molecules. This calculation was based on the signal integration ratios of the amide proton (6.39 ppm) from the P(NIPAM) block, the aldehyde (-CHO) proton (9.80 ppm) from the P(MAEBa) block, and the imine bond proton (11.65 ppm) (Figure 5). Additionally, the ^1H NMR calculation determined the molecular weight of the dopamine-loaded block copolymer to be 13.32 kDa.

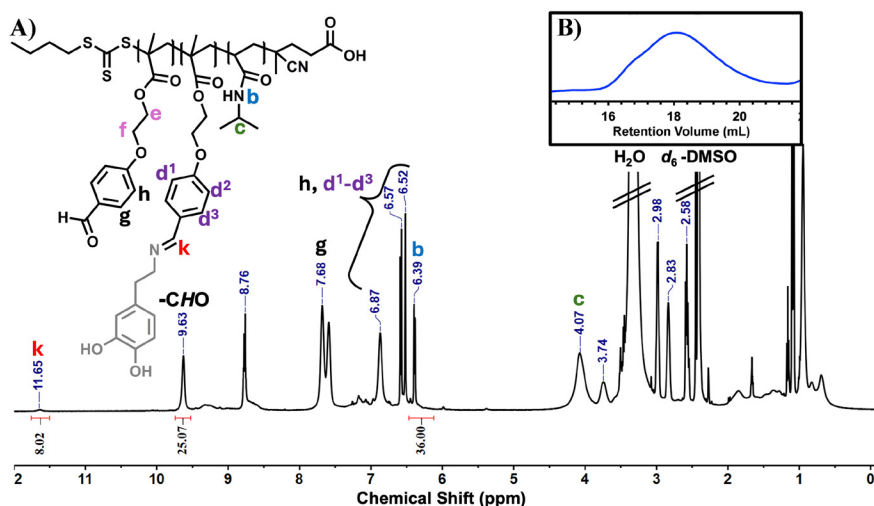


Figure 5. A) ^1H NMR spectrum of P(NIPAM-*b*-MAEBA/DOP) in $\text{DMSO}-d_6$. B) GPC chromatogram of P(NIPAM-*b*-MAEBA/DOP)

As detailed in Table 1, the molecular characterization of the synthesized polymers revealed a shift to higher molecular weights in the GPC distribution after the addition of each block, as illustrated in Figures 3B, 4B, and 5B. Since the GPC system was calibrated with linear polystyrene standards, the GPC

results for all polymers varied significantly from the ^1H NMR findings due to the differing chemical structures.

Table 1. Conversion, molecular weight, and polydispersity indexes (\bar{D}) of polymers

Polymer	^1H NMR ^a		GPC ^b	
	$M_{n,\text{NMR}}$ (kDa)	Conversion (%)	$M_{n,\text{GPC}}$ (kDa)	\bar{D}
P(NIPAM)	4.36	48	1.32	1.25
P(NIPAM- <i>b</i> -MAEBA)	12.09	66	29.45	1.50
P(NIPAM- <i>b</i> -MAEBA/DOP)	13.32	24	30.87	1.76

^aDetermined by ^1H NMR spectrum, ^bDetermined by THF-GPC, polystyrene (PS) standards used for calibration.

Subsequently, a calibration curve ($y=0.01465x+0.00176$, $R^2=0.99941$) for dopamine was plotted by measuring the absorbance values at 280 nm using a UV-Vis spectrophotometer (Figure 6A). The amount of dopamine in the P(NIPAM-*b*-MAEBA/DOP) (1 mg/mL in DMSO) was found to be 78.11 μg via calibration curve (Figure 6B).

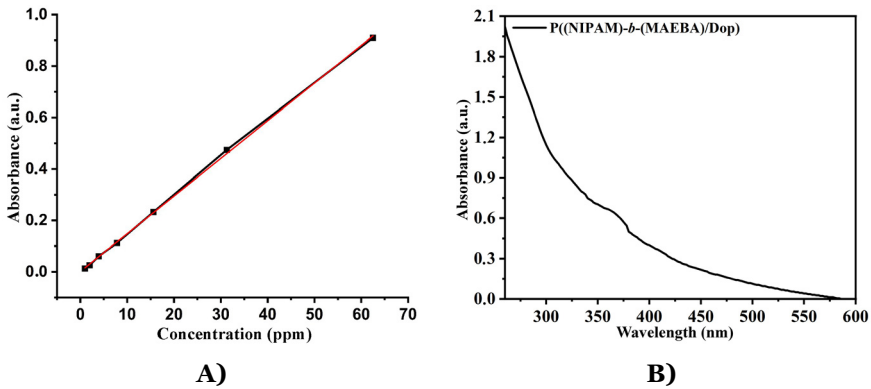


Figure 6. A) Dopamine calibration curve in DMSO and B) UV-Vis spectrum of the P(NIPAM-*b*-MAEBA/DOP) copolymer

An *in vitro* dopamine release assay was conducted using a dialysis method in phosphate-buffered saline (PBS, pH 7.4). A 1 mg/mL polymer solution in DMSO/water (1/3, v/v) was dispersed in PBS and incubated at 37°C for 72 hours. While dopamine release within the initial 10 hours was approximately 18%, a total of 53% of dopamine was released from the polymer over the 72 hours (Figure 7).

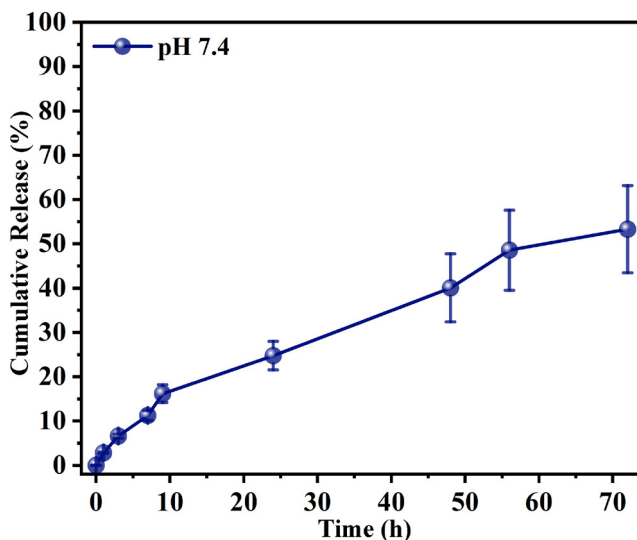


Figure 7. *In vitro* dopamine release profile of P(NIPAM-*b*-MAEBA/DOP) polymer in PBS at pH 7.4 at 37°C

In conclusion, this study developed a potential thermoresponsive and tissue-adhesive platform by synthesizing a block copolymer of P(NIPAM-*b*-MAEBA/DOP) through RAFT polymerization. The spectroscopic and chromatographic analyses confirmed the successful synthesis and structure of both intermediate compounds and the final polymer. This platform exhibited a sustained dopamine release of 53% over 72 hours at pH 7.4. The combination of P(NIPAM)’s well-known thermoresponsive behavior with dopamine’s robust surface adhesion properties suggests this copolymer could be a promising material for various future applications. Its potential applications range from antimicrobial solutions to advanced uses in areas such as implant interfaces, with a significant impact in biomedical fields.

STATEMENT OF ETHICS

This study does not require any ethical permission.

CONFLICT OF INTEREST STATEMENT

The authors have no conflicts of interest to declare.

AUTHOR CONTRIBUTIONS

Concept, design, supervision, and resources, PSOO; data collection and/or processing, IM, BA; analysis and/or interpretation, IM, BA, PSOO; literature search, IM, PSOO; writing, IM, PSOO; critical reviews and supervisions, PSOO.

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REFERENCES

1. Franco R, Reyes-Resina I, Navarro G. Dopamine in health and disease: much more than a neurotransmitter. *Biomedicines*, 2021;9(2):109. Doi: 10.3390/biomedicines9020109
2. Liu Y, Ai K, Lu L. Polydopamine and its derivative materials: synthesis and promising applications in energy, environmental, and biomedical fields. *Chem Rev*, 2014;114(9):5057-5115. Doi: 10.1021/cr400407a
3. Hemmatpour H, De Luca O, Crestani D, Stuart MCA, Lasorsa A, van der Wel PCA, et al. New insights in polydopamine formation via surface adsorption. *Nat Commun*, 2023;14:664. Doi: 10.1038/s41467-023-36303-8
4. Poinard B, Neo SZY, Yeo ELL, Heng HPS, Neoh KG, Kah JCY. Polydopamine nanoparticles enhance drug release for combined photodynamic and photothermal therapy. *ACS Appl Mater Interfaces*, 2018;10(25):21125-21136. Doi: 10.1021/acsami.8b04799
5. Li H, Yin D, Li W, Tang Q, Zou L, Peng Q. Polydopamine-based nanomaterials and their potentials in advanced drug delivery and therapy. *Colloids Surf B: Biointerfaces*, 2021;199:111502. Doi: 10.1016/j.colsurfb.2020.111502
6. Fu Y, Yang L, Zhang J, Hu J, Duan G, Liu X, et. al. Polydopamine antibacterial materials. *Mater horiz*, 2021;8(6):1618-1633. Doi: 10.1039/D0MH01985B
7. Faure E, Falentin-Daudré C, Jérôme C, Lyskawa J, Fournier D, Woisel P, Detrembleur C. Catechols as versatile platforms in polymer chemistry. *Prog Polym Sci*, 2013;38(1):236-270. Doi: 10.1016/j.progpolymsci.2012.06.004
8. He X, Obeng E, Sun X, Kwon N, Shen J, Yoon J. Polydopamine, harness of the antibacterial potentials-a review. *Mater Today Bio*, 2022;15:100329. Doi: 10.1016/j.mtbio.2022.100329
9. Xu Z, Wang T, Liu J. Recent development of polydopamine anti-bacterial nano-materials. *Int J Mol Sci*, 2022;23(13):7278. Doi: 10.3390/ijms23137278
10. Matyjaszewski K. Controlled/living radical polymerization: state of the art in 2002. In: *Advances in controlled/living radical polymerization* [Internet]. American Chemical Society; 2003. p. 2-9. Available from: <https://pubs.acs.org/doi/abs/10.1021/bk-2003-0854.ch001>. [Jun 26, 2003].
11. York AW, Kirkland SE, McCormick CL. Advances in the synthesis of amphiphilic block copolymers via RAFT polymerization: stimuli-responsive drug and gene delivery. *Adv Drug Deliv Rev*, 2008; 60(9):1018-1036. Doi: 10.1016/j.addr.2008.02.006
12. Zhou D, Zhu L, Wu B, Xu Z, Wan LS. End-functionalized polymers by controlled/living radical polymerizations: synthesis and applications. *Polym Chem*, 2022;13(3):300-358. Doi: 10.1039/D1PY01252E
13. Purkait MK, Sinha MK, Mondal P, Singh R. pH-responsive membranes. In: Purkait MK, Sinha MK, Mondal P, Singh R, editors. *Stimuli responsive polymeric membranes* [Internet]. Academic Press; 2018. p. 39-66. Available from: <https://doi.org/10.1016/B978-0-12-813961-5.00002-4>
14. Le Droumaguet B, Nicolas J. Recent advances in the design of bioconjugates from controlled/living radical polymerization. *Polym Chem*, 2010;1(5):563-598. Doi: 10.1039/b9py00363k
15. Asadi N, Del Bakhshayesh AR, Davaran S, Akbarzadeh A. Common biocompatible polymeric materials for tissue engineering and regenerative medicine. *Mater Chem Phys*, 2020;242:122528. Doi: 10.1016/j.matchemphys.2019.122528

16. Ulery BD, Nair LS, Laurencin CT. Biomedical applications of biodegradable polymers. *J Polym Sci Part B: Polym Phys*, 2011;49(12):827-907. Doi: 10.1002/polb.22259
17. Savicke M, Peculyte L, Bendoraitiene J, Samaryk V, Rutkaite R. Thermoresponsive properties of acenaphthylene-labelled chitosan-*graft*-poly(*N*-isopropylacrylamide) copolymers. *Polym Bull*, 2025;82:1893-1914. Doi: 10.1007/s00289-024-05608-z
18. Tao C, Jin M, Yao H, Wang D A. Dopamine based adhesive nano-coatings on extracellular matrix (ECM) based grafts for enhanced host-graft interfacing affinity. *Nanoscale*, 2021;13(43):18148-18159. Doi: 10.1039/D1NR06284K
19. Wang J, Zhu H, Chen G, Hu Z, Weng Y, Wang X, Zhang W. Controlled synthesis and self-assembly of dopamine-containing copolymer for honeycomb-like porous hybrid particles. *Macromol Rapid Commun*, 2014;35(11):1061-1067. Doi: 10.1002/marc.201400029
20. Gu R, Xu WZ, Charpentier PA. Synthesis of polydopamine-coated graphene-polymer nanocomposites via RAFT polymerization. *J Polym Sci Part B: Polym Chem*, 2013;51(18):3941-3949. Doi: 10.1002/pola.2680221.
21. Peng L, Li Z, Li X, Xue H, Zhang W, Chen G. Integrating sugar and dopamine into one polymer: controlled synthesis and robust surface modification. *Macromol Rapid Commun*, 2017;38(3):1600548. Doi: 10.1002/marc.201600548
22. Unver A, Akovali G. Plasma-induced, solid-state polymerization of *N*-isopropylacrylamide. *J Appl Polym Sci*, 2010;115(6):3311-3320. Doi: 10.1002/app.31391
23. Agrawal AK, Jassal M, Vishnoi A, Save NS. Temperature responsive fibers with anisotropic transitional behavior. *J Appl Polym Sci*, 2005;95(3):681-688. Doi: 10.1002/app.21217
24. Mocan M, de Grooth J, Hofman AH, van der Kooij HM, Loos K, de Vos WM. Free-standing thermo-responsive nanoporous membranes from high molecular weight PS-PNIPAM block copolymers synthesized *via* RAFT polymerization. *Polym Chem*, 2017;8(14):2235-2243. Doi: 10.1039/C7PY00023E
25. Sun F, Wang Y, Wei Y, Cheng G, Ma G. Thermo-triggered drug delivery from polymeric micelles of poly(*N*-isopropylacrylamide-co-acrylamide)-*b*-poly(*n*-butyl methacrylate) for tumor targeting. *J Bioact Compat Polym*, 2014; 29(4):301-317. Doi: 10.1177/0883911514535288
26. Qiu L, Hong C, Pan C. Doxorubicin-loaded aromatic imine-contained amphiphilic branched star polymer micelles: synthesis, self-assembly, and drug delivery. *Int J Nanomedicine*, 2015;10(1):3623-3640. Doi: 10.2147/IJN.S78355
27. Li X, Wang L, Chen G, Haddleton DM, Cheng H. Visible light induced fast synthesis of protein-polymer conjugates: controllable polymerization and protein activity. *Chem Commun*, 2014;50(49):6506-6508. Doi: 10.1039/C4CC02277G
28. Zhang J, Peng C. Poly (*N*-isopropylacrylamide) modified polydopamine as a temperature-responsive surface for cultivation and harvest of mesenchymal stem cells. *Biomater Sci*, 2017;5(11):2310-2318. Doi: 10.1039/c7bm00371d
29. Omurtag Ozgen PS, Atasoy S, Zengin Kurt B, Durmus Z, Yigit G, Dag A. Glycopolymer decorated multiwalled carbon nanotubes for dual targeted breast cancer therapy. *J Mater Chem B*, 2020;8(15), 3123-3137. Doi: 10.1039/C9TB02711D
30. Gencoglu Katmerlikaya T, Dag A, Omurtag Ozgen PS, Ersen Cetin B. Dual-drug conjugated glyco-nanoassemblies for tumor-triggered targeting and synergistic cancer therapy. *ACS Appl Bio Mater*, 2022;5(11):5356-5364. Doi: 10.1021/acsabm.2c00749
31. Luan B, Li C, Moad G, Muir BW, Zhu J, Patel J, Lim S, Hao X. Kinetic modelling of the reversible addition-fragmentation chain transfer polymerisation of *N*-isopropylacrylamide. *Eur Polym J*, 2019; 120:109193. Doi: 10.1016/j.eurpolymj.2019.08.020